



APPLICATIONS OF BEHAVIORAL MODELING AND SIMULATION ON LAB-ON-A-CHIP: MICRO-MIXER AND SEPARATION SYSTEM

Y. Wang*, Q. Lin* and T. Mukherjee+

*Dept. of Mechanical Engineering *Dept. of Electrical & Computer Engineering Carnegie Mellon University

http://www.ece.cmu.edu/~mems

Outline



- Introduction and Motivation
- Description of Model and Simulation Framework
- Composable System Simulation
- Summary

Introduction: Biofluidic Lab-on-a-chip



Biofluidic Lab-on-a-chip

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- Sample saving
- Fast and parallel analysis
- High integration and automation

Four subsystems

- Mixer
- Reactor
- Injector
- separation system
- Electrokinetic driven flow
 - Voltage control



Introduction: Electrokinetic Micromixers

Mixing in Microscale

- Low Reynolds number and laminar flow
- Molecular diffusion dominant
- Enhancing techniques
 - Focusing
 - Multi-lamination...



Long mixing channel Long mixing time

Focusing mixer

(Knight, J.B. et al.)

Complex topology geometry/network Extensive design space Arbitrary flow ratio Arbitrary inlet concentration

An important subsystem of lab on a chip



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Method of Composable System Simulation

- A system decomposed into a set of behavioral models
 - **Parameterized**
 - Reusable

Designs formed by interconnecting models



Multi-lamination mixer (Koch, M. et al.)



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Serpentine separation chip (ORNL)

Top-down analysis and design methodology

- Fast and computationally robust
- **Hierarchical system design**





CarnegieMellor Model for Mixing Channels Μ **Fluidic Modeling Model Structure** $c = \sum_{n=1}^{\infty} d_n^{(out)} \cos(n\pi\eta)$ $c = \sum_{n=1}^{\infty} d_n^{(in)} \cos(n\pi\eta)$ $t_{out} = t_{in} + \Delta t$ $\rightarrow t_{out}$ $\rightarrow d_{a}^{(out)}$ $\overline{n=0}$ $d_n^{(out)} = func(d_n^{(in)}, D, w, \mu, L, E)$ $d^{(in)}$ C R Ζ Flow (u) η **Electric resistance and current Convection-diffusion equation E-conductivity** $u\frac{\partial c}{\partial z} = \frac{D}{w^2}\frac{\partial^2 c}{\partial \eta^2}$ $R = \frac{L\sigma}{wh} \qquad \qquad I = \frac{\Delta V}{R}$ **Channel depth Boundary conditions:**

Mixing Time

 $\Delta t = L/u \stackrel{\text{Sample}}{\longleftarrow} electrokinetic \quad t_{out} = t_{in} + \Delta t$ velocity

Concentration coefficients

$$d_n^{(out)} = d_n^{(in)} e^{-(n\pi)^2 \tau} \longrightarrow \tau = \Delta t \cdot D/w^2$$

Dimensionless
diffusion time
Sample diffusivity

$$\left. \frac{\partial c}{\partial \eta} \right|_{\eta=0,1} = 0$$

$$c\big|_{z=0} = \sum_{n=0}^{\infty} d_n^{(in)} \cos(n\pi\eta)$$

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Model for Diverging Intersections





Electric resistance and current

$$R_l = R_r = R_{out} = 0 \qquad I_{in} = I_l + I_r$$

Mixing Time

 $\Delta t = 0 \qquad \qquad t_l = t_r = t_{in}$

Concentration coefficients

Left
stream
$$\begin{cases} d_0^{(l)} = d_0^{(in)} + \sum_{m=1}^{\infty} d_m^{(in)} \sin(\phi_1) / \phi_1 \\ d_{n\neq0}^{(l)} = 2 \sum_{m=0}^{m\neq n/s} d_m^{(in)} (-1)^{n+1} \phi_1 \sin(\phi_1) / f_1 f_2 \\ + \sum_{m=0}^{m=n/s} d_m^{(in)} (1 + \sin(2\phi_1) / (2\phi_1)) \end{cases}$$

Fluidic Modeling



$$C_{l}(\eta) = \sum_{m=0}^{\infty} d_{m} \cdot \cos(ms\pi\eta) \quad c_{r}(\eta) = \sum_{m=0}^{\infty} d_{m} \cdot \cos\left(m\pi(1-s)\left(\eta + \frac{s}{1-s}\right)\right)$$

Splitting position $s = I_{l} / (I_{l} + I_{r})$

$$f_{1} = (m - ns)\pi \qquad f_{2} = (m + ns)\pi F_{1} = (m + n - ns)\pi \qquad F_{2} = (m - n + ns)\pi \phi_{1} = ms\pi \qquad \phi_{2} = m(1 - s)\pi \begin{cases} d_{0}^{(r)} = d_{0}^{(in)} - \sum_{m=1}^{\infty} d_{m}^{(in)} \sin(\phi_{1})/\phi_{2} \\ d_{0}^{(r)} = 2\sum_{m=0}^{m \neq n/(1 - s)} d_{m}^{(in)} \phi_{2} \sin(\phi_{1})/F_{1}F_{2} \\ + \sum_{m=0}^{m = n/(1 - s)} d_{m}^{(in)} (\phi_{2} \cos(\phi_{1}) - \sin(\phi_{1}))/\phi_{2} \end{cases}$$

Basic Models for Separation System

 $L2 = \emptyset$

angle = Ø

Anti-Clockwise

R1 = 100

2 = 11Ø

in

Elbow_2

Basic behavioral models

Name	Description			
Channel	Straight Channel			
elbow_1	Elbow of clockwise flow			
elbow_2	Elbow of anti-clockwise flow			
U_turn_1	Turn of clockwise flow			
U_turn_2	Turn of anti-clockwise flow			

Elbow

out

 $R_2 = 110$

out

 $L1 = \emptyset$

angle = Ø

Clockwise

R1 = 100

 $Elbow_1$

in



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Interface Parameters and Model Structure

Interface parameters

- Variance (σ^2)
- Separation time (t)
- Skew coefficients (B_m)
- Amplitude (A)
- Voltage (V)

Globally determined voltage

- Signal flow of fluidic interface parameters
- Starts from injector
- Simultaneous simulation of two or more species in the analyte



User input

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Component geometry (w, L, R_c) mobility μ and diffusivity D $t_{in} \rightarrow t_{out} = t_{in} + \Delta t$ $B_m^{(in)} \rightarrow B_m^{(out)} = func(B_m^{(in)}, D, w, \mu, L, E)$ $\sigma_{ut}^2 \rightarrow \sigma_{out}^2 = \sigma_{in}^2 + \Delta \sigma^2$ $A_{out} / A_{in} = \sqrt{\sigma_{in}^2 / \sigma_{out}^2}$ V_{in}, V_{out} Kirchhoff's law

Behavioral Model Structure



Input from upstream

Skew coefficients

$$B_m^{(out)} = \pm J\left(1 - e^{-\lambda_m \tau_t}\right) / \lambda_m^2 + B_m^{(in)} \cdot e^{-\lambda_m \tau_t}$$

$$J = 8\theta/\tau_t \qquad \lambda_m = (m\pi)^2$$
$$t = \theta R_c/U \qquad \tau_t = t \cdot D/w^2$$

System Simulations

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DC analysis

- Electric variable (voltage/current)
- Microfluidic simulation
 - Mixing time (t)
 - Conc. profile (*d_n*)
 - Mixing performance
- DC and Transient Analysis
 - Resolution
 - Electropherogram

Verification: Focusing and Multi-stream Mixers

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Verification: Serial Mixing Network

(Jacobson, S.C. et al. Anal. Chem. 1999, 71, 4455-4459)

Waste-2

Concentration comparison

Verification: Double Complimentary Turns

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Verification: Multiple Turns

- Behavioral models used in complex EP system
- Good agreement and tremendous speedup

Serpentine of six turns

Spiral of five turns

Worst relative error 12% compared with experimental results

(C.T. Culbertson, S.C. Jacobson, J.M. Ramsey. *Anal. Chem.* 2000, 72, 5814-5819)

- A composable system simulation framework built for biofluidic lab-on-a-chip
- Behavioral Models implemented in analog hardware description language (Verilog-A)
- Simulation results verified numerically and experimentally (relative error ~< 10%)</p>
- A tremendous speedup (10~15,000X) achieved

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